The Challenges of Out of Position Occupants for Passive Safety in Automated Vehicles

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Bronislaw (Bronek) Gepner Hongnan Lin Taotao Wu Jason Forman Matt Panzer





Background

- Induced a change in <u>occupant position</u>
- Uncertainty in the interaction between the occupant, the <u>restraints</u>, and <u>vehicle</u> <u>interior</u>*









Objectives

- 1. Examine existing <u>crash investigation cases</u> for crashes that involve occupants that were <u>not in a standard automotive seating posture</u>.
- 2. Evaluate the suitability of the existing ATD and human body models to <u>evaluate the kinematics and injury risk for occupants</u> in other than traditional automotive seating postures.







Vehicle Model

- 2012 Toyota Camry (Reicher et al., 2016).
 - Center for Collision Safety and Analysis (GMU)
 - 2.25M finite elements
 - Validated using 10 different full vehicle crash tests
- Major modifications
 - Seat recline angle (3 positions)
 - Seat orientation (5 positions)
 - Vehicle interior



orientation

2012 Toyota Camry



Research Moving Deformable Barrier (RMDB)

- Designed for oblique and small overlap (Saunders et al., 2011)
- Easy to parameterize the multiple impacts
 - 8 crash directions evaluated
- Better simulation stability compared with rigid wall







Restraints

- Airbag models
 - From restrain supplier
 - Passenger airbag (PAB)
 - Curtain airbag (CAB)
 - Side airbag (SAB)
 - Trigger time t = 0ms







Occupant Models

Tissue-level criterion



GHBMC M50-0 (detailed)

Virtual instrumentation







Occupant, Seatbelt Integration

• THOR

Upright seat (25deg)

Semi-reclined seat (40deg)













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Instrumentation and Injury Assessment

Capability of injury assessment for THOR, GHBMC M50-OS and M50-O models

Injury Criteria (reference)	THOR	M50-OS	M50-O
HIC ₁₅ (Versace, 1971)			
BrIC (Takhounts, 2013)			
N _{ii} (Eppinger, 1999)			
cN _{ij} (TBD)			
NIC (Bostrom, 1998)			
Shoulder Load (Petitjean, 2012)			
Clavicle Load (Qi, 2014)			
Multi-point Thoracic Injury Criterion or PCA (Crandall, 2013)			
Rib Strain (TBD)			
Abdomen Compression (Kent, 2008)			
Lateral Shoulder, Chest and Abdomen deflection (Petitjean, 2012)			
Lumbar Spine Load (TBD)			
ASIS Load (TBD)			
Sacral Iliac Load (TBD)			
Acetabulum Load (Martin, 2011)			
Pubic Symphysis Load (Petitjean, 2012)			
Femur Axial Load (Kuppa, 2001)			
Revised Tibia Index (Kuppa, 2001)			
Distal Tibia Axial Force (Kuppa, 2001)			
Proximal Tibia Axial Force (Kuppa, 2001)			

Green: The default model <u>has the</u> <u>required instrumentation</u> to output the injury metric;

Yellow: The default model <u>does not</u> <u>have the required instrumentation</u> to output the injury metric, but we added instrumentation to calculate the injury criteria

Red: The default model <u>is not capable</u> <u>of predicting</u> the injury metric for current modeling method;





Parametric Simulation Suite







Post-processing-Data structure







Automated Vehicle Evaluation Plan

- Study A: Effects of reclining the seat
- Study B: Effects of seat orientation
- Study C: Effects of a turned occupant
- Study D: Effects of having an occupant sleeping on the belt path
- Study E: Effects of having an occupant seated far back from the instrument panel











Simulation Summary

- **175** full vehicle simulations + positioning simulations
- 800,000 core hours of CPU time to run (11 years / 8core machine)
- Output of 477 x 175 channels of instrumentation data
- Output of **3 x 175** videos of the simulations

Termination Results Summary

- 158 of 175 simulations terminated successfully
- Of the 17 simulations in error
 - 7/67 for THOR,
 - 3/95 for M50-OS,
 - 7/13 for M50-0.

Error report		
Occupant model	Part responsible	
THOR	Abdominal block	
	Jacket	
	Upper AB Foam	
M50-OS	Thigh	
	Sacroiliac joint	
M50-O	Pelvis	
	Neck muscle	
	Foot skin	
	Abdomen muscle	





Outstanding Issues for M50-OS

• Unrealistic flesh sliding off of the pelvis





Reclined M50-OS, standard seatbelt, frontal impact

Note:

Substantial shear force resulting in the sliding over and around the pelvis. This has a substantial effect on submarining response.





Outstanding Issues for M50-OS

- Unrealistic internal organ response and flesh response
- Failure to maintain internal cavity volume



Semi-reclined M50-OS, standard seatbelt, rear impact

Note:

- M50-OS model lacks a continuity definition between flesh, skeleton and underlying organs.
- Pelvis flesh stuck in the crease between seat cushion and back deformed a lot.





Positioning

Stability

Lessons Learned (simulation study)

- Positioning seat in vehicle
- Occupant fit for non-frontal facing

Interference issues – non-trivial

- ► GHBMC-M50 spine too stiff for natural settling
- **GHBMC-M50-O** is stiffer than M50-OS during positioning
- ▶ THOR cannot go fully reclined (only ~40 deg) Dummy design issue
- ► GHBMC_M50_OS abdomen causing negative volume
- Unrealistic internal cavity organs' connection for GHBMC_M50_OS
- **•** THOR face flesh deforms substantially during simulation
- ▶ M50-OS is more stable than THOR FE
 - Non reinforced seatback deforms under rear impact





Forward-facing, upright seat with standard seat belt, frontal impact

Comparison between M50-OS and M50-O



M50-OS

- Neck flexion →M50-O has larger neck flexion compared with M50-OS.
- Pelvis kinematics→M50-OS slides forward, tilts back more than M50-O.







Forward-facing, upright seat with standard seat belt, frontal impact

- M50-OS has larger flexion in the thoracic spine, and engages PAB
- M50-OS engages knee bolster earlier (initial position and longer thighs)
- THOR does not engage PAB well, and has large cervical spine flexion as a result
- THOR pelvis has less motion than M50-OS
- THOR head hits roof at windshield

Loadcase 1 : Time = 0.000000 : Frame 1 M50-OS_Upright_0_Std_0_RMDB



Loadcase 1 : Time = 0.000000 : Frame 1 THOR_Upright_0_Std_0_RMDB







Forward-facing, semi-reclined with integrated belt, frontal impact

Comparison between M50-OS and M50-O



 Neck flexion →M50-O has larger neck flexion compared with M50-OS.

 Pelvis kinematics→M50-OS slides forward, tilts back more than M50-O.







Forward-facing, semi-reclined with integrated belt, frontal impact

- THOR semi-reclined: 40°
- M50-OS semi-reclined: 45°
- M50-OS engages knee bolster earlier (initial position and longer thighs)
- Neither model engages PAB well
- THOR has larger cervical spine flexion compared to M50-OS
- THOR pelvis has less motion than M50-OS

Loadcase 1 : Time = 0.000000 : Frame 1 M50-OS_Semirecline_0_Int_0_RMDB



Loadcase 1 : Time = 0.000000 : Frame 1 THOR_Semirecline_0_Int_0_RMDB







Forward-facing, reclined seat with integrated belt, frontal impact

Comparison between M50-OS and M50-O



- Neck flexion →M50-O has larger neck flexion compared with M50-OS.
- Pelvis kinematics→M50-OS slides forward, tilts back more than M50-O.





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Pelvis Motion and Submarining Response - M50-OS vs M50-O

Reclined seat (60deg)

Semi-reclined seat (45deg)

Upright seat (25deg)





M50-OS











Pelvis Motion and Submarining Response - M50-OS vs M50-O vs THOR

Semi-reclined seat (45deg)



Upright seat (25deg)

1. LS-DYNA keyword deck by LS-PrePos

2.1 SJDVNA kerwood dark hv I SJDvaDost

Loadcase 1 : Time = 0.000000 : Frame 1

1 LS-DYNA keyword deck by LS-PrePost

Loadcase 1 : Time = 0.000000 : Frame 1

Londonne 1 : Time = 0.000000 : Frame 1

GHBMC M50 Full Body Model: Occupant

Loadcase 1 : Time = 0.000000 : Frame 1

2 LS-DYNA keyword deck by LS-PrePost Loadcase 1 Time = 0.000000 Frame 1

2 LS-DYNA keyword deck by LS-PrePost

Loadcase 1 : Time = 0.000000 : Frame 1



Lessons Learned (simulation study)

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 - THOR cannot go fully reclined (only \sim 40 deg) – Dummy design issue
 - GHBMC M50 OS abdomen causing negative volume
- Unrealistic internal cavity organs' connection for GHBMC_M50_OS
- THOR face flesh deforms substantially during simulation
- Stability M50-OS is more stable than THOR FE
 - Non reinforced seatback deforms under rear impact
- Restraint THOR FE pelvis rotates opposite direction compared to GHBMC (frontal impact)
 - GHBMC-OS shows greater lap belt penetration into abdomen than GHBMC-O



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